ABSTRACT

The management of segmental bone loss remains as an unsolved controversy. Bone defects after traumatic injuries are related to poor functional outcomes and prolonged periods of recuperation. In the management of large bone defects the selection of the adequate bone graft requires a deep acknowledgment of the advantages and disadvantages of each bone substitute available. Autologous bone grafts remain the gold standard to measure all of the available bone substitutes; the ideal bone substitute must provide properties such as osteoconduction, osteoinduction and the osteogenic property, it must also be readily available, provide mechanical support, manageable, biocompatible, provide a sufficient amount of substitute according to the situation and it has to be bioresorbable. We present the case of a patient with a large (>5 cm) diaphisal defect of the tibia managed with a single, large bone block harvested from the iliac crest and its evolution after a one year follow up.

KEY WORDS

Bone Grafts; Posttraumatic Bone Defect; Bone Substitutes; Autografts; Allogeneic Bone Grafts; Ceramics; Bioactive Glass.

CASE SERIES

Bone formation can be defined as the process that results from the coordinated interaction between an appropriate substrate, growth factors and osteogenic cells. Despite the first two cited elements are already available in artificial preparations, the same affirmation cannot be applied to the source of osteogenic cells that can only be found in bone autografts [1, 2].

When assessing the selection between the different available options for bone grafting, autologous bone graft remains the gold standard to compare all others bone substitutes [3-5]. Autografts usually suffer from less resorption derived from their histocompatibility properties, the presence of viable cells and their osteoconductive and osteoinductive properties [6]. The autografts lack the risk of transmitting infectious diseases and are available at no cost [7].

The ideal graft must provide specific properties in the best combination to achieve bone growth, including: osteoconduction which refers to the ability of a graft to provide an adequate environment for bone formation and capillary ingrowth, osteoinduction: the capacity to recruit pluripotent mesenchymal stem cells that differentiate into osteoblasts and chondroblasts, osteogenic property which implies that the graft contains viable osteocytes or precursors. The ideal graft must also be readily available, manageable, provide mechanical support, biocompatible and bioreasorbable [7-10].

In some situations bone autografts are not available or do not provide a sufficient quantity to fill a large bone voids. Bone substitutes such as demineralized bone matrix, morselized and cancellous allografts ceramics and ceramics composites have osteoconductive properties and in some cases (morselized and cancellous allografts, osteochondral and cortical allografts) can provide mechanical support. They lack the osteogenic property of iliac crest autografts [7, 11, 12].

We present the case of a patient with a large (>5 cm) diah
phiseal defect of the tibia managed with large bone block harvested from the iliac crest and its evolution.

**CASE REPORT**

Figure 1: Initial X-rays, antero-posterior view.

Figure 2: Initial X-rays, lateral view.

A 22-years old male, with no medical comorbidities, presented to the clinic after being managed for six months in other center for a tibial shaft fracture secondary to a firearm injury. He was initially managed with wound debridement and the application of an external fixator in the operating room. After a 6-month follow-up he was told he had a tibial non-union and needed a second surgery. The initial evaluation showed an afebrile patient with stable vital signs, without abnormalities in the thoracic and abdominal evaluation. He entered the clinic walking with the help of two crutches, and a monoplanar external fixator device in the left leg with four pins along the anterior tibial margin. None of the pins presented with loca infection signs at the site of insertion. There was a marked muscular atrophy of the left leg. An anterior scar of about 2 cm wide in the mid-shaft tibial region with no infection signs was visible. Sensation, pulses and distal capillary refill showed no abnormalities. Radiographs showed a displaced multiftamentary tibial shaft fracture (AO 42C-3). The external fixator was removed one week prior to surgery.

Figure 3: X-rays after external fixation removal, anteroposterior view.

Figure 4: X-rays after external fixation removal, lateral view.

He was taken to the operating room where open reduction and internal fixation with a LCDCP 4.5 mm plate with the implantation of a tricortical iliac crest bone graft was performed.

**Surgical technique**

In the Operating Room, with sterile technique, an anterior approach to the tibial shaft was used exposing the site of the fracture evidencing several large necrotic fragments of the tibial shaft without signs of infection and presence of abundant fibrotic tissue. The avascular fragments were removed until finding bleeding bone leaving a segmental tibial shaft defect of 10 cm with an oblique proximal margin and a transverse distal margin.

A second approach to the iliac crest was performed to obtain a tricortical iliac crest autograft. A segment of 11 cm long was obtained. The ends of the graft were molded to be fitted in the medullary cavity of the proximal and distal fragments.

The fracture was fixed using a LCDCP 4.5 mm plate with 4 cortical screws in the proximal tibial fragment and 4 cortical screws in the distal fragment. The autograft was fixed to the plate with 2 cortical screws and an additional 3.5 mm cortical screw was placed to increase the stability in the oblique margin of the proximal shaft fragment. The wound was irrigated and closed.

Figure 5: Postoperative X-Rays, antero-posterior view.

Figure 6: Postoperative X-Rays, lateral view.

**RESULTS AND DISCUSSION**

The patient reported early development of pain at the donor site requiring the prescription of analgesics that resolved after four weeks.

After a 12 month follow up the patient shows a consolidation rate of 100% between the distal margin of the autograft and the tibial shaft and a rate of 85% between the proximal margin of the autograft and the tibial shaft. The patient tolerates full weight bearing and walks with one crutch.

Figure 7: X-rays after external fixation removal, anteroposterior view.

Figure 8: X-rays after external fixation removal, lateral view.
POST TRAUMATIC BONE DEFECTS

The surgical management of segmental bone loss remains as an unsolved controversy between orthopaedic surgeons. Treatment of extremities with multifragmentary fractures may be complicated by segmentary bone loss and damage to the soft tissue coverage. The challenge becomes even more complex when fibrosis and alteration of regional irrigation arises [13, 14]. Aggressive debridement of bone in multifragmentary open fractures reduces the risk of infection creating in exchange a posttraumatic segmental bone defect. Most authors recommend the removal of contaminated or avascular bone fragments and soft-tissue attachments. Performing an insufficient debridement will increase the risk of leaving contaminated tissues that can lead to chronic infection [14, 15].

The treatment of patients with bone loss is commonly associated to poor functional outcomes and prolonged periods of recuperation [16, 17]. When assessing the decision-making process, the knowledge about advantages and disadvantages for the different available surgical techniques and the different methods to manage soft tissues to create an environment that facilitates bone regeneration, play a crucial role in achieving the therapeutic goals [13, 18].

The treatment must be aimed to achieve a stable and functional extremity in the shortest, most tolerable way for the patient. Up to now, we have several available surgical techniques for handling segmental bone loss: Induced membrane technique, free vascularized autogenous bone graft, bone transport and distraction, demineralized bone matrix, non-structural and structural autologous bone graft between others [17, 20]. These options may be supplemented with the use of demineralized bone matrix or bone morphogenetic protein [16, 21, 22].

Table 1: Types of bone grafts.

<table>
<thead>
<tr>
<th>Types of bone grafts</th>
<th>Properties</th>
<th>Presentations</th>
<th>Mechanical Support</th>
<th>Disadvantages</th>
</tr>
</thead>
<tbody>
<tr>
<td>Autologous bone grafts</td>
<td>Osteoinduction</td>
<td>Cancellous, Cortical or corticocancellous grafts</td>
<td>-Depending of the type.</td>
<td>-Donor site morbidity</td>
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<td></td>
<td>Osteoconduction</td>
<td></td>
<td></td>
<td>-Limited supply</td>
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<td></td>
<td>-Osteogenic</td>
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<tr>
<td>Allogeneic bone Grafts</td>
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</tr>
<tr>
<td>Demineralized bone matrix</td>
<td>-Osteoconduction</td>
<td>Commercial preparations including paste, mix, strip, inject and putty</td>
<td>-They can provide mechanical support depending of the shape of the defect.</td>
<td>-Risk of infectious diseases</td>
</tr>
<tr>
<td></td>
<td>-Osteoinduction (arguable)</td>
<td></td>
<td></td>
<td>-slower integration</td>
</tr>
<tr>
<td>Osteochondral and cortical allografts</td>
<td>-Osteoconduction</td>
<td>Whole bone or joint.</td>
<td>Provide mechanical support</td>
<td>-Higher Risk of infectious diseases</td>
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<td></td>
<td></td>
<td></td>
<td></td>
<td>-Slow integration</td>
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<tr>
<td>Ceramics and ceramics composites</td>
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<tr>
<td>Calcium Phosphate</td>
<td>-Osteoconduction</td>
<td>Block, granular, powder or putty form</td>
<td>No mechanical support</td>
<td>Little tensile strength.</td>
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<tr>
<td>substitutes</td>
<td></td>
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<tr>
<td>Calcium Sulfate</td>
<td>-Osteoconduction</td>
<td>Powder</td>
<td>No mechanical support</td>
<td>Slow integration</td>
</tr>
<tr>
<td>Bioactive Glasses</td>
<td>-Osteoconduction</td>
<td>Microspheres Fibers</td>
<td>No mechanical support</td>
<td>Variable rates of integration according to formulation.</td>
</tr>
<tr>
<td>Silica, calcium oxide, disodium oxide and pyrophosphate in different formulations</td>
<td>-Osteoconduction</td>
<td>Microspheres Fibers</td>
<td>No mechanical support</td>
<td></td>
</tr>
</tbody>
</table>
In order to achieve bone formation there are five requirements considered mandatory for uneventful consolidation: osteogenic cells, an osteoconductive scaffold, growth factors, a stable mechanical environment and vascularity [10, 23].

**Autologous bone grafts**

The use of autologous bone grafts in the management of segmental bone loss is considered a useful tool for its osteoinductive and osteoconductive capacity becoming a biological stimulus for bone healing and regeneration, the grafts also provide with osteogenic cells to the site of implantation [9, 13, 24]. The iliac crest is the most common donor site for bone grafts, it can provide a large volume of autografts of different types (cancellous, cortico-cancellous, unicortical, bicortical or tricortical segments). Cancellous autografts can be harvested from this location preserving its trabecular architecture, this specific type of autograft does not provide mechanical stability. It is rapidly incorporated into the host site due to its osteogenic properties, the large area it provides for bone formation and the abundance of growth factors [25]. Cancellous bone grafts have the additional advantage of providing functional osteoblasts at the site of desired regeneration. The surviving osteocytes combined with graft porosity and local inflammatory response factors promote angiogenesis and recruitment of mesenchymal stem-cells that can differentiate into osteoblasts. New bone formation allows for the graft to completely turnover by one year. Autogenous cortical bone graft is a reliable option to achieve structural stability with or in the absence of a bone void, it provides an osteoconductive medium and immediate mechanical stability. Cortico-cancellous grafts offer the advantages of cancellous bone grafts (rapid integration, source of new osteoblasts, osteoinduction, osteoconduct) and the advantages of cortical autogenous bone grafts (mechanical stability) [8, 26].

Although in some publications the general recommendation is not to manage bone voids larger than 5 cm with autogenous grafts [4, 26]. The use of non vascularized autogenous bone grafting for larger segmental bone defects (up to 16 cm) has been described to provide satisfactory results in several case series [14, 25, 27-29] (Figure 1).

In the case presented, we had a satisfactory functional outcome with the use of a single, iliac crest, block of 10 cm to manage the tibial defect. The bone segment appears to have recovered circulation on the 12 month follow up X-rays, despite its size.

In patients that need more grafts than the quantity than can be supplied via autograft augmentation or patients with high risk of developing complications from autograft harvesting, other options should be considered for bone grafting such as allografts or synthetic bone fillers. The surgeon must make a decision based on the deep knowledge of the properties and weakness of each allograft or bone substitute. The availability of the substitute and the personal experience with the materials should be considered as important factors.

**Donor Site Morbidity of Bone Autografts of the Iliac Crest**

Complications associated to harvesting of bone grafts in the anterior iliac crest can be divided into major and minor. Minor complications are those that required no or minimal treatment and resulted in minimal disability whereas major complications are those that required repeated surgical intervention, readmission, and prolonged hospital stay or resulted in significant long term disability. Minor complications include persistent pain at donor site, superficial sensory nerve injury, superficial hematoma or seroma, superficial infection. Major complications are such as deep hematoma requiring surgical treatment, vascular injury, sacroiliac joint injury, ureteral injury, donor site fracture, incisional hernia, trendelenburg gait, deep infection [8, 20, 30]. The frequency of such complications are variable between studies. Arrington reported in retrospective review of 414 cases a frequency of 10% minor complications and 5.8% mayor complications [30]. Younger informed an overall rate of major complications of 8.6% (infection, prolonged wound drainage, large hematomas, reoperation, pain greater than 6 months, sensory loss, and unsightly scars) between 239 medical records reviewed [31]. Goulet studied 192 cases of autogenous iliac crest bone harvesting reported 21.8 % (37 patients) with minor complications and 2.4 % (4 patients) with major complications [32]. Cockin reported a rate of minor complications of 6% and a rate of major complications of 3.4% in a series of 118 iliac crest bone grafts [33]. The incidences vary depending the inclusion criteria for minor and major complications.

Related to the size of the harvested graft there has been studies that reported complications such as incisional hernia associated to the use of tricortical iliac crest bone grafts [8, 34, 35]. Some studies suggest that the larger the size of the graft, the higher the risk of major complications [34, 35].

The patient of our case reported early development of pain at the donor site. This complaint required the prescription of analgesics for approximately four weeks. We did not suffer any mayor complications despite the size of the harvested graft.

**Allogeneic Bone**

Allogeneic bone is available in many preparations including: demineralized bone matrix, morselized and cancellous chips, corticocancellous and cortical grafts and whole bone segment [7, 36].
Deminerlized bone matrix acts as an osteoconductive material and it has arguable osteoinductive properties [8, 9, 36]. Its osteoinductive property relies on the presence of proteins and growth factors, which can vary between donors and with a variable preparation process [8, 9, 37].

Morselized and cancellous chips are considered osteoconductive and can provide some mechanical support. They are associated to a small risk of transmitting infectious diseases [8, 38].

Osteochondral and cortical allografts are available as a whole bone or joint for limb salvage in large bone defects. They are osteoconductive, variably osteoinductive and carry a small risk of transmitting diseases, depending on their treatment and processing. The risk is increased when fresh allografts are used. In a clinicopathological study of retrieved human allografts, Enneking found that the union at cortical-cortical junctions occurs over a period of 12 months or more and the bone gap filled does not undergo stress-oriented remodeling, even after several years, thus failure occurred at this junction when the disruption was performed [38]. In other observational study on massive retrieved human allografts the findings of slow integration and osteoconductive rather than osteoinductive property of allografts were also reported [39].

**Ceramics and Ceramics Composites**

Synthetic bone graft substitutes consist of hydroxyapatite, tricalcium phosphate, calcium sulfate or their combinations [10, 41]. When attached to vascularized bone, osteoid is produced into the surfaces of the ceramic without formation of an interface of soft tissue [23]. Although the unlimited supply, easy sterilization and storage can be cited as their strong points, their disadvantages include brittle handling properties, variable rates of resorption, poor performance in diaphyseal defects, and potentially adverse effects on normal bone remodeling [40, 41].

Calcium phosphate substitutes are osteoconductive synthetic bone fillers with no osteoinductive property unless osteoinductive substances (BMP, growth factors) are added resulting in a composite graft. They provide no structural support and have little tensile strength. Calcium phosphate ceramics include hydroxyapatite, coralline hydroxyapatite, tricalcium phosphate an biphasic calcium phosphate [8-10, 42].

Tricalcium phosphate is a frequently used resorbable ceramic. It can be obtained in different presentations: block, granular, powder or putty form. It provides limited biomechanical support due to lower tensile resistance [8-10, 42].

Hydroxyapatite is available in non-absorbable or absorbable solid forms as granules. Its bioreosorption is related to its manufacturing process and it is mediated by macrophages, or giant cells [10, 42].

Degradation of tricalcium phosphate and calcium phosphate cement is done by osteoclasts in a period of time of about 1 year; hydroxyapatite degrades in a period of approximately 2-5 years. Tricalcium phosphate ceramic is removed as bone ingrowth is produced while hydroxyapatite is more permanent [23, 41, 42].

Coralline hydroxyapatite is based on certain coral species which produce a porous structure of calcium phosphate similar to human cancellous bone with osteoconductive properties as a bone substitute with high compressive resistance but brittle at low tensile strength [23, 42].

Calcium-collagen graft substitute is a composite of hydroxyapatite, tricalcium phosphate and type I and III collagen mixed with autologous bone marrow to provide its osteogenetic property. It does not provide structural support and can be used to augment fracture healing in acute cases [7, 23, 42].

Calcium sulfate is a substitute available in a dry powder form, it is considered osteoconductive with no osteoinductive or osteogenetic property. It is completely dissolved in a period of 6-12 weeks. Its main use is to replace bone after tumor resections [10, 42].

The use of hybrid grafting (β- tricalcium phosphate and demineralized bone matrix) for larger defects has also been reported, with high levels of success [43]. The disadvantages of this method include the availability of the grafts and the high cost.

**Bioactive Glasses**

Bioactive glasses are synthetic bone substitutes composed mainly of silica, calcium oxide, disodium oxide and pyrophosphate. They are available in the presentations of porous implants, microspheres and fibers. After implantation they bind to collagen, growth factors and fibrin to form a matrix that allows bone ingrowth by infiltration of osteogenic cells. The resorption rate of these materials depends on variations on their formulation. The matrix does not provide structural support despite its capacity to support some degree of compressive strength [7, 23, 44].

**CONCLUSION**

The management of posttraumatic segmental bone defects requires a thorough awareness of the advantages, disadvantages and singular properties of every option available for induce bone ingrowth or substitution, as well as the specific conditions and characteristics provided by the patient (age, comorbidities, weight, habits, etc) and the injury (contamination, infection, size of the defect, mechanism, etc.). Bone autografts remain the gold standard in bone grafting, they account for the principal properties to be sought on a bone substitute (osteoinduction, osteoconduction, osteogenetic property).
REFERENCES


